Registration of Positron Emission Tomography (PET) Image and Functional Near Infrared Spectroscopy (NIRS) Data

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Abstract: Functional near infrared spectroscopy (NIRS) is the optical imaging that measures changes of blood hemodynamic while positron emission tomography (PET) measure physiological condition of the interest area. NIRS has high temporal resolution while PET image has better spatial resolution compared, however, NIRS measures hemodynamic changes in the cortex region but not in deeper brain structures. Therefore, this study is aimed to register the both image; the NIRS data on the PET image. The registration of NIRS on PET image was done on eleven subjects which undergoes NIRS and PET scan separately. To register the NIRS probe on the PET image, we did a transformation of NIRS probe coordinate to the PET coordinate based on Polaris marker position attached to the NIRS cap. The coordinate of these markers is obtained using the optical tracking system, Polaris. The resulting image forms PET and NIRS were visually aligned as well as the coordinate of the marker obtained during the PET acquisition. The probe was registered on the PET image using the in-house software. The registration done in this study is considered successful as we can view the NIRS activation area on PET image.

Key words: Functional near-infrared spectroscopy, PET-NIRS, multimodal image registration.

1. Introduction

In recent years, medical image registration has gained considerable attention to gather as much information as possible for the diagnosis of the disease. Calvin Maurer (1993) defined the image registration as the determination of one-to-one mapping between the coordinates in one space and those in another such that points in the two space that correspond to the same anatomical point are mapped to each other [1]. The goal of image registration is to align the images with respect to each other, match the corresponding images based on certain features to assist in the image fusion and to produce as output geometrical transformation that aligns corresponding points and can serve as input to a system further along in the image acquisition [1], [2].

Recently, there has been many modalities in radiology as well as nuclear medicine where each of them

has their own purpose and advantages. To optimize the advantages of each modality, multimodal imaging is available to help a better diagnose. This lead to the multimodal image registration which is matching images of the same patient which acquired by different imaging technologies. Normally the registration image is in between integration of anatomical and functional image. Most common multimodal image registration is magnetic resonance imaging (MRI) and positron emission tomography (PET), PET and computed tomography (CT), single photon emission computed tomography (SPECT) and CT.

This paper focuses on registering the functional near-infrared spectroscopy (NIRS) on positron PET image. This is a multimodal image registration which used a hardware-based system as the references. Basically, NIRS and PET are the imaging modalities that give functional information, especially for brain activity.

Near infra-red spectroscopy is the optical imaging system that used near infra-red light to assess the functional state during brain activities. It can detect changes in the concentration of oxygenated and deoxygenated hemoglobin in blood [3]. The change in hemodynamic response is a good marker for assessing neural activity since the oxygenated level is dependent on brain activities and mostly NIRS measurement is done based on mental work in human [4]. NIRS measured the oxygenated level of blood, which similar to blood-oxygen-level dependent (BOLD) technique in fMRI. Nevertheless, the beauty of NIRS is it can detect the oxygenated changes while the subject is doing an activity. In view of the fact that NIRS is task related, there are many studies done involves NIRS measurement while the subject is doing a task such as an exercise using muscle [5], [6], playing a video game system [7], cycling [8] and verbal fluency task [9], [10].

PET is nuclear imaging technique that used radioactive to image the functional state inside the human body. It is involving the injection of a radiotracer into human body where the tracer is a biological compound of interest labelled with a positron emitters isotope such as 11 C, 18 F and 15 O [11]. Specific tracers are chosen to illustrate the particular brain functions, for example, 18 F-2-deoxyglucose (18 FDG) is used to investigate cerebral glucose metabolism, whereas H_2^{15} O is used to examine cerebral blood flow [11].

Both techniques NIRS and PET, have their own advantages and disadvantages. NIRS has high temporal resolution while PET image has a better spatial resolution [12]. NIRS also is relatively non-invasive technique, inexpensive compared to other modalities, safe in term of radioactive usage and portable. NIRS is completely silent, providing a nonintrusive environment and allowing for an easy presentation of auditory stimuli [13]. However, the depth penetration of light in NIRS is very low, therefore NIRS only measures hemoglobin concentration on the cortex region rather than in deeper brain structures [13], [14]. Thus, brain structures that lie deeper in the cortex or below it is not visible using NIRS techniques [13].

Therefore, by registering the NIRS data on PET image, it can optimize the advantages of NIRS and PET as well as improve the specificity of the information given by both methods. This paper describes how the process of registration of NIRS on PET image using hardware base registration.

2. Materials and Methods

2.1. Study Design

This study was done at Cyclotron and Radioisotope Center (CYRIC) Tohoku University. Fig. 1 illustrates the process to register the NIRS on the PET image. PET image is used as the reference image while NIRS data as the target image and the registration is based on a hardware-based system which is done using Polaris. NIRS data is relatively the probes location on the NIRS cap. Each subject undergoes NIRS examination and PET scanned separately and therefore Polaris markers were attached on NIRS cap as in Fig. 2a and subject wore the cap for both procedures. To register the NIRS on PET image, we transformed the NIRS probe location into the PET coordinate based on the Polaris marker location.

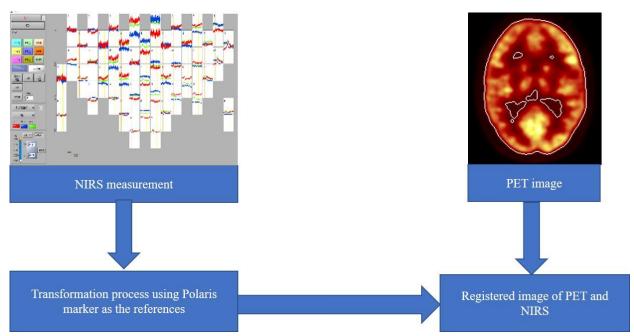


Fig. 1. The process to register the NIRS on PET image using Polaris marker as the reference. The NIRS measurement is undergoing transformation process beforehand register on PET image.

2.2. Participants

A total of eleven subjects participated in this study. All subject is male and healthy subject (age 20 to 25 years old). Subject with brain abnormalities was excluded from this study. Written consent was obtained from each subject before undergoing this experiment.

2.3. Functional Near Infra-Red Spectroscopy

During the NIRS task, the changes of hemodynamic response in the prefrontal cortex were recorded by NIRS FOREI 3000 system (Shimadzu Inc., Kyoto Japan). This NIRS system consists of transmitting probe which emits infrared light at three different wavelengths (780, 805 and 830 nm) and receiving probe which record the reflected infrared light. The probe is mounted on the NIRS cap and separate 3 cm apart each. The NIRS cap was fixed on subject head over the prefrontal regions and the location of NIRS probe was determined using FASTRAK 3D magnetizer.

2.4. Positron Emission Tomography (PET)

PET scanner used in this study was Eminence STARGATE PET-CT scanner (Shimadzu Inc., Kyoto, Japan). As this study only focuses on PET, we only used PET scanner instead of CT function. The scanning covered only brain part, which is about 5 minutes transmission scan for tissue attenuation correction and 20 minutes emission scan.

2.5. Optical Tracking System

The optical system used in this study was Polaris Vicra NDI as shown in Fig. 2b. Polaris use near infra-red to detect the 3D location of markers. It has two digital cameras that can detect location and orientation of multiple markers simultaneously. Polaris marker is made of the material that can reflect the infra-red light so that Polaris can detect the reflected light. Fig. 2a shows the sticker type marker while Fig. 2c shows the ball type Polaris marker. In this study, we used sticker type marker to attach on the NIRS cap while ball type marker was attached to the PET gantry.

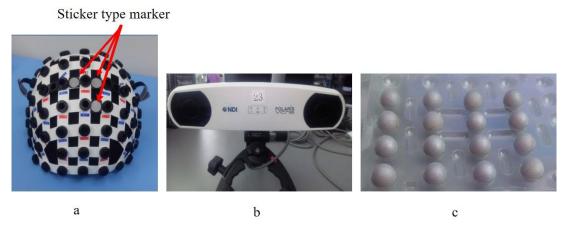


Fig. 2. a) The sticker type Polaris marker that attached to the subject cap b) The Polaris Vicra NDI and c)

The ball type Polaris marker that used on the gantry.

2.6. Measurement Procedures

The whole procedure is shown in Fig. 3. The details of this study are found in elsewhere [15]. Before the preparation for the NIRS examination, the subject was inserted with normal saline drip into the left antecubital vein. Then the subject was asked to sit comfortably on the chair facing the PC monitor during the fixation of the NIRS cap. Three Polaris markers were attached to the NIRS cap as in Fig. 3 and subject wore the cap for both procedures. Since the NIRS and PET are done separately, the cap was fixed tightly on the subject head to prevent movement during the transition PET room later. Before fixing the NIRS probe, the location of all NIRS probes was determined using FASTRAK 3D magnetizer. After fixing all the NIRS probe on the cap, FDG-18 was injected into the subject through the left antecubital vein. The NIRS task started shortly after the injection and subject completed the task within 30 minutes as well as NIRS measurement. After the task finished, all the NIRS probes were removed from the cap and the subject was transferred to the PET room with the cap still on the subject head. Then the subject was laid out on the PET bed and the head is fixed to immobilize during the scanning. The setup is shown in Fig. 4. At the same time, Polaris is placed in between the PET gantry and CT gantry as shown in Fig. 4a. Polaris is connected to a personal computer and read the position of Polaris marker on the cap as well as the gantry marker during the PET scanned (Fig. 4b).



Fig. 3. The flow of the procedure of the measurement.

2.7. The Registration

The registration process started with the transformation of NIRS probe and Polaris marker to the PET coordinate. The transformation process is illustrated in Fig. 5. Considered we have three coordinate systems:

1) NIRS; C_{NIRS} 2) Polaris system; C_{POL} and 3) PET image; C_{PET} . From the measurement done, we have coordinate of the probe, P_{NIRS} (x, y, z) in C_{NIRS} given by magnetic probe and the coordinate of marker M_{POL} (x, y, z) in C_{POL} given by Polaris. The transformation is done to convert these coordinate into C_{PET} . The transformation is divided into two steps, first is the conversion of P_{NIRS} (x, y, z) to the C_{PET} and second is the conversion of M_{POL} (x, y, z) into C_{PET} . The P_{NIRS} (x, y, z) was transformed to the P_{POL} (x, y, z) in C_{POL} using transformation matrix; $T_{NIRS-POL}$ as the beforehand transformed to P_{PET} (x, y, z) in P_{PET} using transformation matrix; P_{POL} (Fig. 5). The marker P_{POL} (x, y, z) in P_{PET} (Fig. 5). The details of these transformation are given in the appendix. Thereafter, registration of the NIRS probe, as well as Polaris marker on the PET image was done. The transformation process gave the NIRS probe position in PET coordinate, P_{PET} . By using in-house software, we did register the NIRS coordinate and Polaris marker on the PET image.

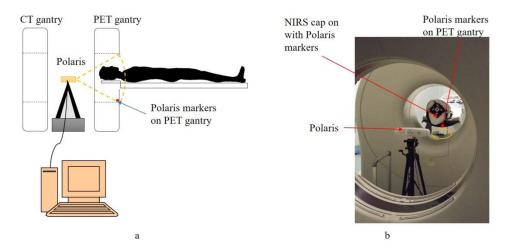


Fig. 4. a) Illustration of the Polaris and subject set up. The Polaris placed in between CT and PET gantry and connected to a personal computer system for the data recording. b) The position of the subject head as well as Polaris. Three Polaris markers are attached to the cap and three markers on PET gantry.

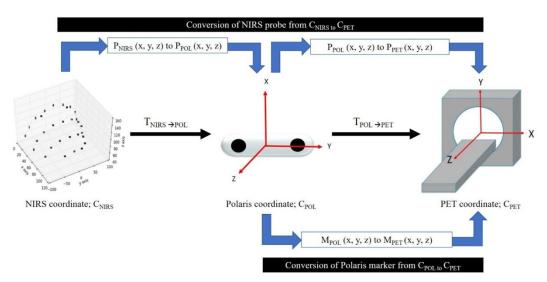


Fig. 5. The entire flow of transformation process. The 30 probes were transformed to Polaris coordinate beforehand transformed to C_{PET} , while the Polaris markers were transformed directly to C_{PET} .

3. Result

The transformation of the probe from C_{NIRS} to C_{POL} done for all eleven subjects by using Kabsh algorithm [16]. The transformation matrix $T_{NIRS-POL}$ was calculated for each subject individually. The $T_{NIRS-POL}$ was calculated form conversion of M_{NIRS} to M_{POL} and error of each subject was determined. Seven subjects out of eleven subjects give error less than 1 mm, while another four subjects give error below than 5 mm. The error was calculated by comparing the estimated M_{POL} coordinate using calculated $T_{NIRS-POL}$ and the actual value M_{POL} coordinate. For the transformation from C_{POL} to C_{PET} , the transformation matrix was determined by transformed the 22 Na position given by Polaris to the known position of 22 Na on PET image. Therefore, for all subject, the transformation from Polaris to C_{PET} were based on only one value of T_{POL} PET. Fig. 6 shows the activation area based on NIRS task which is view on PET image. The NIRS task consists of three tasks, therefore, we can view the activation area on PET image for the task 1, task 2 and task 3 such in Fig. 6a, 6b and 6c.

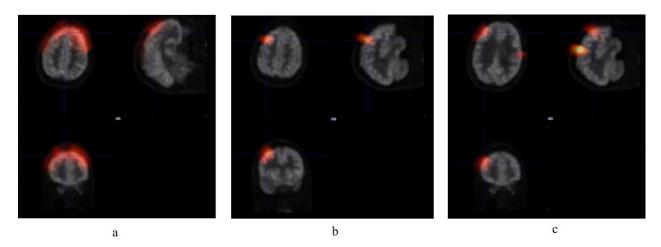


Fig. 6. The activation area based on NIRS task which observed on PET image. The red colour shows the activation area during NIRS task. a) The activation area during the first task, b) The activation area during the second task and 3) The activation area during the third task.

4. Discussion

We demonstrated the registration of NIRS on PET image for all eleven subjects using geometrical transformation methods. The aim of this study is to register the NIRS image on PET image, therefore the result is focused on the translation of the NIRS probe coordinate and Polaris marker coordinate to the PET coordinate. The registration of NIRS on PET image is considered successful and we can view the NIRS activation area on the PET image. The NIRS measurement depends on the length of the light travel, thus NIRS result is mostly in the cortex region of the brain. Thus, by transformed the NIRS probe to the brain surface of PET image, we can see clearly where the changes happened during the task performed. As the task in this study is the cognitive task, therefore the response is in the frontal area as shown in Fig. 6.

Our approach is to bring the NIRS on PET together to optimize the information given by NIRS and PET alone. NIRS alone can detect the change of oxyhemoglobin and deoxyhemoglobin in blood during brain activity. The activation of the brain related to the changes of blood flow to the active area and changes of oxyhemoglobin and deoxyhemoglobin in blood [4]. Therefore, NIRS is very beneficial when measures during brain activity. Several NIRS studies in demonstrated that changes in brain activity can be assessed non-invasively [17]. There are several types of brain activity have been assessed during motor activity, visual activation, auditory stimulation and performance of cognitive task [8], [17]. Meanwhile, ¹⁸FDG-PET is used to investigate cerebral glucose metabolism wherein certain activated brain regions, the demand for

glucose and oxygen may increase due to the increased regional brain energy metabolism. Therefore, performed PET scan after the NIRS task could visualize the active area where high glucose uptake due to the NIRS task. Despite the fact that NIRS has a critical issue on spatial resolution, but then it gives a good temporal resolution. On the other hand, PET produces better spatial resolution compare to NIRS. Therefore, this work could give better consequence where we can view the activation area during NIRS task on PET image.

In this study, the registration technique is done base on extrinsic method [18]. We use Polaris marker as the artificial object attached on the subject and this technique also is hardware base registration where we used Polaris as the optical tracking system to register both images. However, there is an error on the transformation matrix from NIRS to PET for a certain subject. This error is probably due to the movement of the cap during the transfer from NIRS room to PET room and this cause rotation of the marker on the cap although we already fix the cap tightly to reduce the movement.

Our technique is the initial phase to produce a better fusion between NIRS and PET as the registration is the first step of image fusion [2]. Recently, there are many approaches of multimodal imaging such as PET-CT, MRI-CT and PET-MRI [2], [19], [20]. Generally, all these multimodal images have more advantage as it gives information anatomical and physiological and more clinical benefits [1]. However, PET-CT technique involves large radiation dose as the patient receive radiation from radiotracer injected during PET as well as x-ray from CT [21]. For the PET-MRI or CT-MRI, those technique is costly compared to NIRS which is considerably lower. Thus, for those who already have PET machine, the installation of NIRS will be less expensive compared to installing the CT or MRI.

Another technique similar to our study is PET-fMRI as the BOLD technique of fMRI also monitor the oxygen level in blood. However, NIRS can detect the change of oxyhemoglobin, deoxyhemoglobin as well as total hemoglobin in blood while the BOLD response in fMRI only is related to deoxyhemoglobin only [13]. Another advantage is NIRS is task related, so that we can visualize the hemodynamic level change during task and NIRS is completely silent, provide a nonintrusive environment and allowing for an easy presentation of auditory stimuli [13].

Recent work on NIRS with combination other imaging technique are done simultaneously. NIRS is a freely moving tool, therefore the combination of NIRS-PET or NIRS-fMRI done simultaneously where the NIRS tools are brought to the bedside and subject performed the task during both measurements [22]-[24]. Although NIRS is portable and can bring along to the bedside in PET or MRI room, the task is limited due to space and a complicated setup is required for simultaneous measurement. These will lead to inconvenience during the task done and probably contribute the motion in PET. In our approach, the NIRS and PET are done separately, give more space and comfortable environment during the NIRS task and then go for PET scan with less motion during the scanning.

This work has the limitation as well. As the PET and NIRS are done separately, the subject was required to wear the NIRS cap for a longer time such in this study for one hour. Although the cap is soft, it may bring uncomfortable for certain subject especially elderly or child. Besides that, the registration may take time as the transformation is done for each subject. In future, a standard software should be developed for the effectiveness of the registration process.

5. Conclusion

This registration of NIRS on the PET image is considered successful but then again, this registration technique should be tested on another object such as phantom to validate this registration method. This study is relatively new, but then it is a respectable jump to make a better fusion image of NIRS and PET. The main challenge of NIRS-PET fusion is the need to visualize deeper in the brain structure since brain

activities not only in the cortex region. In future, clinical aspect should be considered in order to gain as much clinical information as well as provide a better diagnosis and to expand the patient benefits.

Appendix

The transformation of the NIRS cap, P_{NIRS} (x, y, z) and Polaris marker; M_{POL} (x, y, z) to the C_{PET}.

1) Conversion of P_{NIRS} (x, y, z) into C_{POL}

Based on probe coordinate given by magnetic probe, we calculated the coordinate of the marker in the C_{NIRS} . The marker location, M_{NIRS} (x, y, z) in C_{NIRS} is corresponded to the marker location, M_{POL} (x, y, z) in C_{POL} , as shows in the following relationship;

$$M_{POL} = T_{NIRS} \rightarrow_{POL} * M_{NIRS}$$

Therefore, $T_{NIRS \rightarrow POL}$ is given by the following relationship;

$$T_{NIRS \rightarrow POL} = M_{POL} * M_{NIRS}^{-1}$$

By using $T_{NIRS \rightarrow POL}$, coordinate of probe, P_{POL} (x, y, z) in C_{POL} was calculated by the following equation;

$$P_{POL} = T_{NIRS} P_{POL} * P_{NIRS}$$

2) Conversion of $P_{POL}(x, y, z)$ and $M_{POL}(x, y, z)$ into C_{PET}

The coordinate of probe, P_{POL} (x, y, z) and marker, M_{POL} (x, y, z) in C_{POL} is corresponded to P_{PET} (x, y, z) and M_{PET} (x, y, z) in C_{PET} , as given by the following relationship;

$$P_{PET} = T_{POL \triangle PET} * P_{POL}$$
 and $M_{PET} = T_{POL \triangle PET} * M_{POL}$

To calculate the $T_{POL}_{\rightarrow PET}$, we did an experiment using sodium point source (^{22}Na) to get the position of Polaris marker in PET coordinate as well as Polaris coordinate. This experiment was setup same as in PET scanning and Polaris measurement setup except that ^{22}Na source was put on the PET couch. The ^{22}Na source was surrounded by Polaris markers so that we get the source position in C_{POL} as well as in C_{PET} . Thus, the coordinate of $^{22}Na_{POL}$ (x, y, z) in C_{POL} is corresponded to $^{22}Na_{PET}$ (x, y, z) in C_{PET} as in the following relationship;

22
Na _{PET} = T_{POL} \rightarrow PET * 22 Na _{POL}

Therefore, $T_{POL_{\rightarrow}PET}$ is given by the following relationship;

$$T_{POL \rightarrow PET} = {}^{22}Na_{PET} * {}^{22}Na_{POL} - 1$$

By using $T_{POL \rightarrow PET}$, coordinate of probe, PPET (x, y, z) in C_{PET} was calculated by the following equation; $P_{PET} = T_{POL \rightarrow PET} * P_{POL}$ as well as coordinate of marker coordinate; $M_{PET} = T_{POL \rightarrow PET} * M_{POL}$

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Conflict of Interest

H. Watabe and M. Tashiro have potential conflicts of interest regarding the grant from GlaxoSmithKline.

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